

U.S. PATENT APPLICATION

FOR

5 METHOD FOR MATCHING AND REGISTERING MEDICAL IMAGE DATA

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CROSS-REFERENCE TO RELATED APPLICATIONS

This application is cross-referenced to and claims priority from U.S Provisional Application

15 60/414,104 filed 09/27/2002, which is hereby incorporated by reference.

STATEMENT REGARDING FEDERALLY SPONSORED RESEARCH OR DEVELOPMENT

The present invention was supported in part by grant number RO1 CA72023 from the National Institutes of Health (NIH/NCI). The U.S. Government has certain rights in the
5 invention.

FIELD OF THE INVENTION

The present invention relates generally to medical imaging. More particularly, the present invention relates to methods for matching and registering medical imaging data based on
10 anatomical similarity.

BACKGROUND

Computed Tomographic Colonography (CTC) is a minimally invasive method for the examination of the colon using spiral/helical CT volume data. The standard imaging
15 process includes colon cleansing and air-insufflation, followed by CT imaging of the abdomen while the patient is in the supine position. However, insufficient cleansing and air-insufflation often cause some parts of the colon wall to be covered with water (See e.g. S.C. Chen et al., "CT colonography: value of scanning in both the supine and prone positions," *Am J Roentgenol*, vol. 172(3), pp. 595-599, 1999; J.G. Fletcher, et al.,
20 "Optimization of CT colonography technique: prospective trial in 180 patients," *Radiology*, vol. 216(3), pp. 704-711, 2000; J. Yee, et al., "The usefulness of glucagon hydrochloride for colonic distention in CT colonography," *Am J Roentgenol*, vol. 173(1), pp. 169-172,

1999). Furthermore, retained solid fecal material can mimic a polyp in CT images (See e.g. J.G. Fletcher et al., "CT colonography: potential pitfalls and problem-solving techniques," *Am J Roentgenol*, vol. 172(5), pp. 1271-1278, 1999 (With comments in *Am J Roentgenol*, vol. 172(5), pp. 1179, 1999)). These limitations are largely overcome by imaging the colon a second time with the patient in the prone position. The radiologists then compare the two sets of images to assess for movement of feces and to examine surfaces hidden in supine position. This requires careful anatomic alignment between the two data sets. However, as the patients change position, their colons deform and may stretch or shrink in length. Currently, anatomic matching the two data sets is tedious and time consuming. Accordingly, there is a need for a more convenient and automatic method that would allow matching of these two data sets.

SUMMARY OF THE INVENTION

The present invention provides an automatic method for the registration of prone and supine Computed Tomographic Colonography (CTC) data. The method improves the radiologist's overall interpretation efficiency as well as provides a basis for combining supine/prone computer-aided detection results automatically. In general, the method matches and registers medical image data obtained from different perspectives or taken at different times. The medical image data could be obtained from other organs or (tubular) structures other than the colon such as blood vessels or airways, other areas of the gastrointestinal tract, and solid structures or organs that can be segmented, such as bones.

Once the medical images are obtained, e.g. supine or prone data of the colon, the method determines centralized paths or axes of the colon. The method then determines relatively

stationary points, referred to as landmarks, along the centralized axis/path of the colon for both supine and prone positions. In one aspect, these landmarks are local extrema (minima and maxima along the path). These landmarks typically relate to known and automatically identifiable anatomical points or flexures of the colon and are used to match the data sets.

5 Stretching and/or shrinking of either the supine or prone centralized path perform the registration of these landmarks. The stretching and/or shrinking could be performed in a linear or a non-linear fashion. The stretching and/or shrinking could be performed using one or more local extrema, n-th order derivations, curvatures, or the like. The method could be performed on either one of the x, y, z axis or any combination or order of these

10 axes. The matching occurs in an iterative and recursive manner and is considered successful based on one or more decision criteria.

BRIEF DESCRIPTION OF THE FIGURES

The objectives and advantages of the present invention will be understood by reading the following detailed description in conjunction with the drawings, in which:

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FIG. 1 shows an example of a 3D view of prone (a) and supine (b) colon images from one patient, which were segmented using fixed threshold intensity, according to the present invention;

FIG. 2 shows an example in which arrows **210**, **220**, **230** and **240** show possible landmark locations and a centralized path **250** that the method of the present invention is capable of locating automatically;

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FIG. 3 shows an example of a colon centerline path, both supine (solid line) and prone (dashed line), as three functions of x , y and z coordinates versus path length originated from the anus;

FIG. 4 shows an example of supine data (410 z_s) and prone data (420 z_p) before the registration and the supine data (415, dashed line) after it was matched/registered onto the prone data. The bold points on the curves show the local extrema (landmarks) that were identified and used for matching automatically; and

FIG. 5 shows an example of the colon centerlines for a supine (510) and prone (520) data with five anatomically identical points marked on each by a radiologist. The mapping between the two centerlines before (530) and after (540) the matching, in terms of the equal distance to the rectum along the centerlines, is also shown. It is clear that the matching method of the present invention achieves close correspondence between anatomically identical points (the correspondence between the 4th anatomically identical points is shown).

DETAILED DESCRIPTION OF THE INVENTION

Although the following detailed description contains many specifics for the purposes of illustration, anyone of ordinary skill in the art will readily appreciate that many variations and alterations to the following exemplary details are within the scope of the invention.

Accordingly, the following preferred embodiment of the invention is set forth without any loss of generality to, and without imposing limitations upon, the claimed invention.

Colon wall segmentations for both the 3-dimensional (3D) prone and supine CT data were generated using seeded region-growing at a fixed intensity threshold (**FIG. 1**). From the segmented colon, centralized paths through the colon were computed using a 3D medial axis transform, for instance sampled at 1mm intervals, and stored as x , y , and z coordinates

5 (See e.g. D.S. Paik et al. 1998, "Automated flight path planning for virtual endoscopy", Medical Physics 25 (5), 629-637) (**FIG. 2**). The centralized paths could also be computed with another method known in the art. Instead of using a centralized path, one could also use a path that can be obtained in a fairly consistent manner from the data sets. It would be preferred that the resulting (centralized) path is a fairly smooth path. In case the computed

10 (centralized) path still contains a certain amount of noise, this noise could be filtered out with any type of digital filter known in the art.

The x , y , and z coordinates of the centralized path were used as the inputs to the matching and registration method. As a convention, the $+z$ axis is from feet to head, the $+x$ axis is

15 from the left side of the patient to the right side, and the $+y$ axis from posterior to anterior (See **FIG. 2**). Distances along the centralized path and the coordinates could be defined as relative to the initial path point at the anus **260**.

The path coordinates of supine data (x_s , y_s , z_s) and prone (x_p , y_p , z_p) are functions of the

20 distance along the centralized path, d . **FIG. 3** shows an example of these six functions for a single patient. An important observation at this point is that x_s , y_s , z_s resemble x_p , y_p , z_p respectively in terms of their morphologies, but not at the location along the centralized

path d . It is therefore the objective of the present invention to compare and match the data according to landmarks such as their anatomical feature and location on the respective centralized paths. Once correspondence between the landmarks is matched, linear and/or non-linear operations can be applied so that the matched landmarks coincide along the path.

- 5 The description *infra* focuses on the z axis for the sake of simplicity, though the method can be similarly applied to any individual (or combination of) axis (axes).

The morphological similarity between z_s and z_p can be observed as a similarity between the number of landmarks, such as local extrema used in this particular example (LoP; including
10 local minima or local maxima), and their order in terms of their z values as shown in **FIG. 4**. If one sorts the LoP's with respect to their z values, the LoP's of z_s and z_p with equal or close indices are more likely to correspond to the same anatomical points along the central paths. In anatomical terms, LoP's correspond to the deflection points of the central path of the colon and are used as landmarks for the method. It is noted that the method is not
15 limited to the use of local extrema since other landmarks could be used such as n -th order derivations, curvatures, or the like.

Despite of the fact that these deflection points may move within the 3D volume (patient's abdomen) between supine and prone scans, they remain to be deflection points with (small)
20 shifts in their locations to d . Furthermore, LoP's with larger z coordinate values typically correspond to relatively more stable anatomic points. They also correspond to the points further away from the anus **260**, for example, LoP's with highest z values are the most

superior locations in the colon. Anatomically these points typically correspond to the hepatic 210 and splenic 220 flexures (FIG. 2). These relatively fixed flexures are the endpoints of the much more mobile transverse colon. It is noted that LoP's along the other axes correspond with different anatomical points. In general, we have observed that
 5 between prone and supine scans the colon generally deviates less in z- than the y- or x-axis, and the colon is more likely to deform in y-axis than other two axes (i.e. misalignment between supine and prone data set).

The path matching method is based on coupling LoP's for the x-, y-, and z- axes. In a
 10 specific example, the path registration method is based on coupling of LoP's of z_s and z_p and registering their positions with respect to d by segmental stretching and/or shrinking of one of the two paths. The method is not limited to using the supine or prone data set as a reference to match the prone or supine data set respectively.

15 The first step is baseline adjustment of the two paths. It is assumed that the beginning and the ending point of the two paths (spPt and prPt) correspond to the same anatomical points, the anus and the tip of the cecum. Let the path length functions of the spPt and prPt be $D_s(i) = i, i \in [1, N_s]$ and $D_p(i) = i, i \in [1, N_p]$ respectively. A linear transformation, T , is applied such that:

$$20 \quad D_p(1) = \hat{D}_s(1) = T(D_s(1)) \quad (1)$$

$$D_p(N_p) = \hat{D}_s(N_s) = T(D_s(N_s)) \quad (2)$$

This is equivalent to taking the first and last point of the two paths as two pairs of coupled LoP's of spPt and prPt and registering them with respect to d . The z values along the spPt are also changed linearly such that $z_s(1) = z_p(1)$ and $z_s(N_s) = z_p(N_p)$. Note that the linear transformation, T , is the mapping between spPt and prPt. It will be modified in the subsequent steps in a nonlinear fashion to yield to final piecewise linear mapping function.

The second step is to determine the LoP's. The landmarks (local extrema) of $z_s(\hat{D}_s)$ and $z_p(D_p)$ are determined using numerical derivation and neighboring extrema are clustered such that the minimum distance along the path between two consecutive clusters is for instance 15 mm. The mean location along the path and the mean z value for spPt and prPt (LoP_s's, i.e. LoP's on the supine data, and LoP_p's, i.e. LoP's on the prone data, respectively) are used. These identified LoP_s's and LoP_p's are ordered with respect to their z values and indexed. **FIG. 4** shows the LoP_s's and LoP_p's for z_s and z_p .

The next step is to find the LoP_s, LoP_p pair most likely to correspond to the same anatomical point. The decision criteria are based on the differences between their z values and their locations along the path.

$$i, j \in \{1, 2\} \text{ and} \quad (3)$$

$$\left| \hat{D}_s(\text{LoP}_s(i)) - D_p(\text{LoP}_p(j)) \right| < 100 \text{ mm} \quad (4)$$

$$K < \hat{D}_s, D_p < L \quad (5)$$

where i and j are indices assigned to LoP's in the region of interest (ROI, defined by (5)) only with respect to their z values. Condition (3) forces the algorithm to match LoP's starting from the ones furthest away from the anus, i.e., the ones most likely to correspond to anatomical landmarks (like the hepatic and splenic flexures). Condition (4) is a constraint in the maximum stretching/shrinking allowed. In this example this maximum is set to 100 mm, however the maximum allowed stretching/shrinking could also be smaller or larger than 100 mm. Condition (5) defines the boundaries of ROI on which the registration is applied. Initially, $K = D_p(N_p) = \hat{D}(N_s)$ and $L = D_p(1) = \hat{D}(1)$. Then a linear stretching/shrinking operation is applied to \hat{D}_s such that:

$$T(\hat{D}_s(LoP_s(i))) = D_p(LoP_p(j)) \quad (6)$$

The method matches the right and left hand sides of the matched point recursively, for a pre-specified level of recursions or until it could not find any pair of LoP's that satisfy the above criteria. The recursive matching and registration algorithm could be summarized as follows:

1. Perform baseline correction
2. Find LoP's
3. Initialize recursion_level = 0 and K and L to set ROI
4. Sort and index LoP's in ROI
5. If recursion_level < max_recursion_level AND a pair of LoP's and LoP's are matched based on equations (3), (4), (5)

- a. Update \hat{D}_s , based on equation (6)
- b. Increase recursion_level by 1
- c. $K_0 = K, L_0 = L$
- d. Set $K = \hat{D}_s(LoP_s(i)) = D_p(LoP_p(j))$
- 5 e. Go to step (4) (process right hand side)
- f. Set $K = K_0, L = \hat{D}_s(LoP_s(i)) = D_p(LoP_p(j))$
- g. Go to step (4) (process left hand side)
6. Output \hat{D}_s

10 The method described *supra* for the z axis can be similarly applied to x and y axes exactly in the same way. The order in which the axes are considered can be iterated until it converges to a final \hat{D}_s or for a pre-specified number of iterations. It will be clear that the number of axes can be selected as well as the order or the selected axes.

15 The present invention has now been described in accordance with several exemplary embodiments, which are intended to be illustrative in all aspects, rather than restrictive. Thus, the present invention is capable of many variations in detailed implementation, which may be derived from the description contained herein by a person of ordinary skill in the art. For example, the method is also applicable to path comparison and matching of other

20 tubular structures such as blood vessels or airways, other areas of the gastrointestinal tract, and to solid structures that can be segmented such as bones. In addition, the method can be applied to other types of imaging data such as magnetic resonance imaging and ultrasound. Other possible variations to the current method and implementation relate to the fiducial point determination and pair-wise matching which could use the curvature and position

25 information. The method could further be extended and refined by inclusion of several

other types of information, such as torsion, estimated anatomical location, or the like. Another variation is that the piece-wise linear operations performed for matching can be refined by using non-linear operations. For example, the segments corresponding to the transverse colon can be registered by linear operations whereas nonlinear mappings can be used for the segments corresponding to the rectum. In one example, coupling is achieved by copying the most current mapping to other axes and matches/registers a segment at a time while keeping the other segments fixed. The iterative and recursive nature of the method can be extended by further including the information from axes and segments other than the one being registered, at the time of registration. All such variations are considered to be within the scope and spirit of the present invention as defined by the following claims and their legal equivalents.